

Research Seminar

Tianjin University of Technology

辅助康复机器人感知控制 Advanced Sensing and Control of Assistive/Rehabilitative Robots

陈小奇 教授

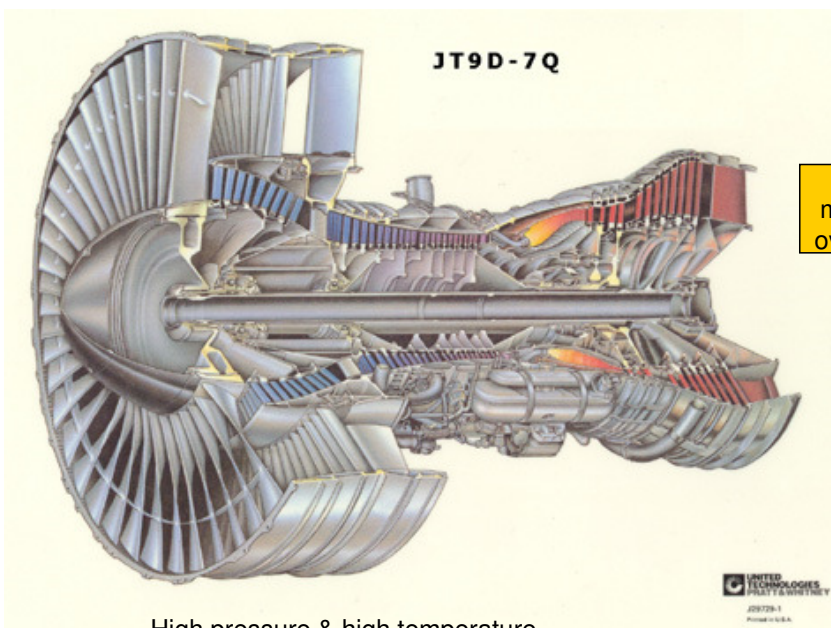
新西兰 坎特伯雷大学 (Univ. of Canterbury)

机械工程系, 机械电子工程实验室

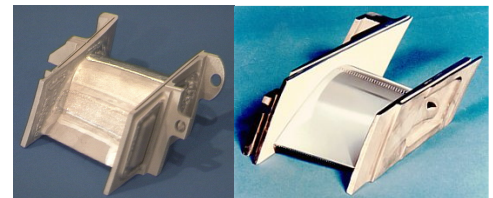
2015年1月19日

Advances in Factory Automation

Aero Engine High Pressure Turbine
(HPT) Airfoil Overhaul



High pressure & high temperature
operating environment up to about
1900F & 190PSI



*HTP vane before
& after blending*



*Compressor
blade before &
after blending*

Repair,
maintenance &
overhaul (MRO)



*HPT blade
before & after
Blending*

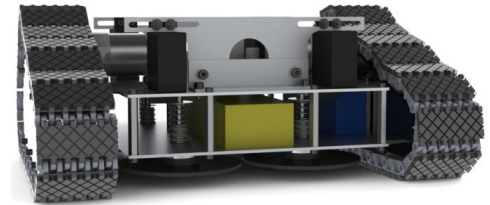
Untethered Wall Climbing Robot 无拴线爬壁机器人

Hidden microbes in weld cracks
can taint millions of litres of milk !

(在焊缝裂纹隐藏的微生物可以玷污
百万升牛奶！)



INVERT
ROBOTICS



6 person team,
6 hour inspection
process with
safety concern



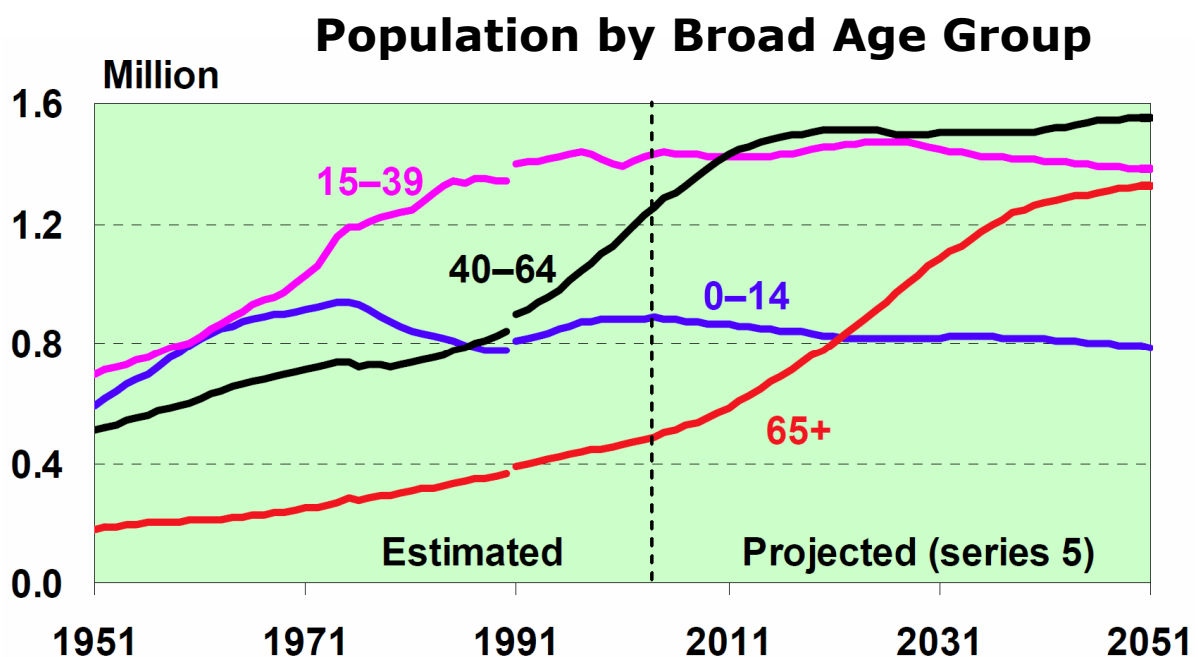
1 operator, 0.5
hour inspection,
operating
outside tank



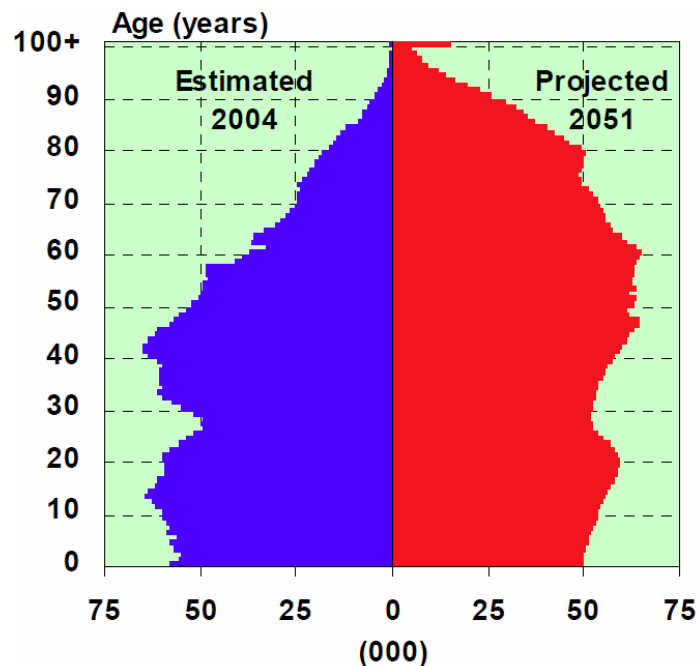
Powered Assistive Exoskeleton

- [背景介绍](#)
- [外骨骼系统, 肌电传感器](#)
- [气动人工肌肉和模糊控制系统](#)
- [实验](#)
- [结论](#)

Motivation-Ageing Population



Age Distribution of Population



Demographic Aspects of New Zealand's Ageing Population, March 2006 .

Motivation

- Cost of intensive medical care
 - **6000/yr (NZ), 2/3 will require rehabilitation**
 - **\$25000/person**
- Decrease recovery time- constant usage
- Better form of assistance for lower limb
- Other possible application where force augmentation is necessary

Motivation-Advancements in Technology



Motivation-Improvement on current form of assistance



Walking Aids



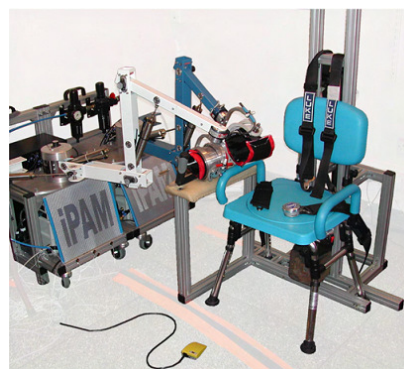
Motivation - Other possible applications



Upper Limb Assistive Devices



ARMin: Tobias Nef et al.(2007)



iPAM: A. Jackson et al.(2007)



MIT-MANUS: Hermano Igo Krebs et al.(2007)

Upper Limb Assistive Devices

- UC Arm Skater, Chen XQ (2009)



- Min force: 4N
- Max force: 22.5N
- Force delivered omni-directionally
- Accurate force control, limited by omni wheel slip

Lower Limbs - Related Work

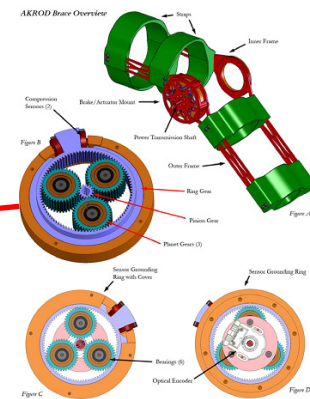
- Michigan state university, Daniel P Ferris et al- Ankle foot Orthosis
- Delivers force to ankle joint for plantarflexion and dorsiflexion
- The study aimed to analyze if mechanical assistance at the ankle joint would reduce the metabolic cost level for steady speed walking-Result it does but not significant enough because of the recoil action of the Achilles tendon.
- The study was mainly concerned with in house testing of the effects of powered exoskeleton on human gait.



Daniel P. Ferris et al. (2008)

Lower Limbs - Related Work

- Active Knee Rehabilitation Orthotic Device(AKROD)- Northeastern University
- Electro-rheological fluid in the knee joint provides variable resistive damping to assist in knee control during swing
- Limitation- Does not provide torque to the joint but rather active dampening



Weinberg B et al.(2007)

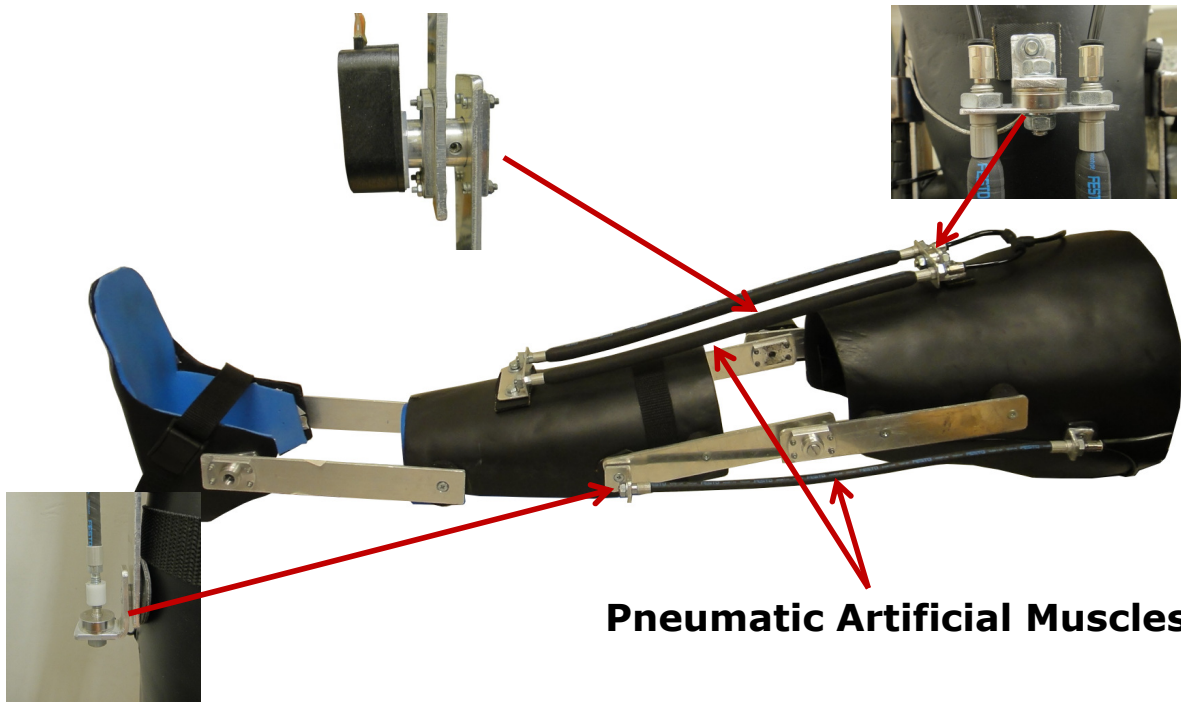
Objectives

- An active lower limb exoskeleton for assistance and rehabilitation
- Pneumatic Artificial Muscles (PAM) for actuation
- Using control signals derived in real time from the user- Surface electromyography (sEMG) and joint kinematic information
- Augment the force produced by the user's skeletal muscle

Prototype

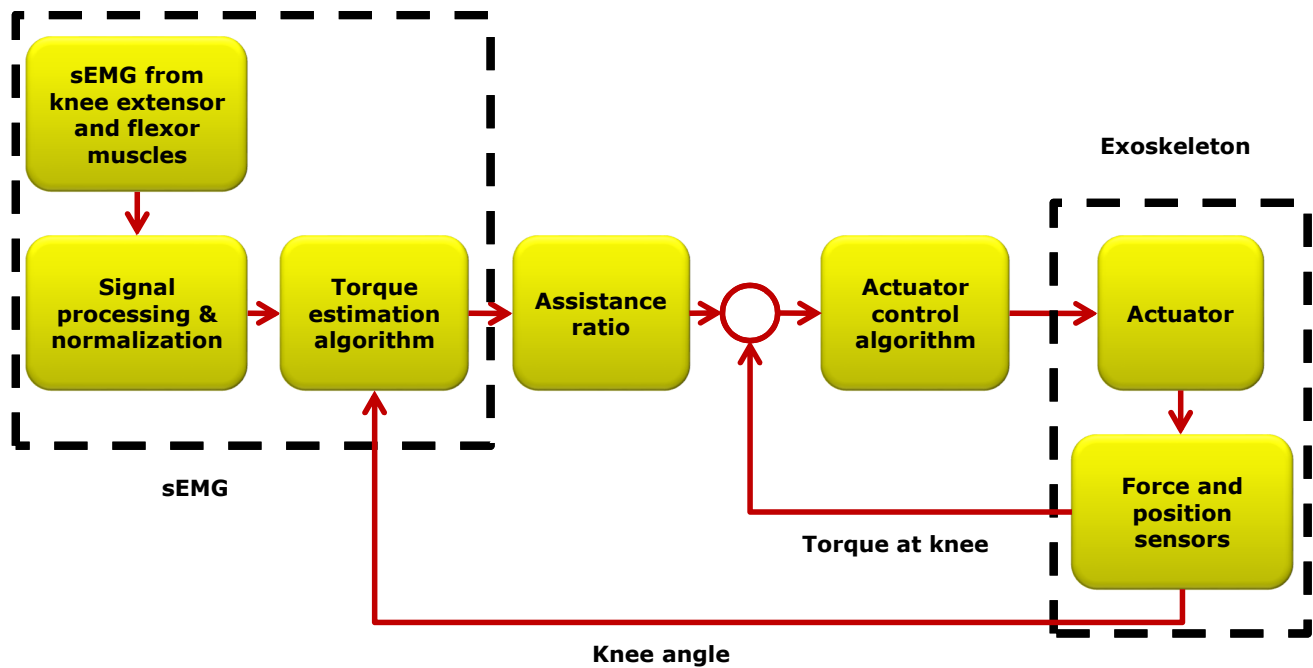


Exoskeleton hardware-Prototype

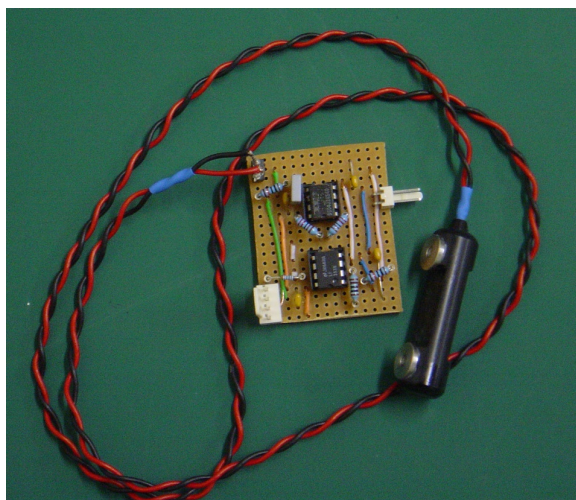


Pneumatic Artificial Muscles

Exoskeleton System Overview

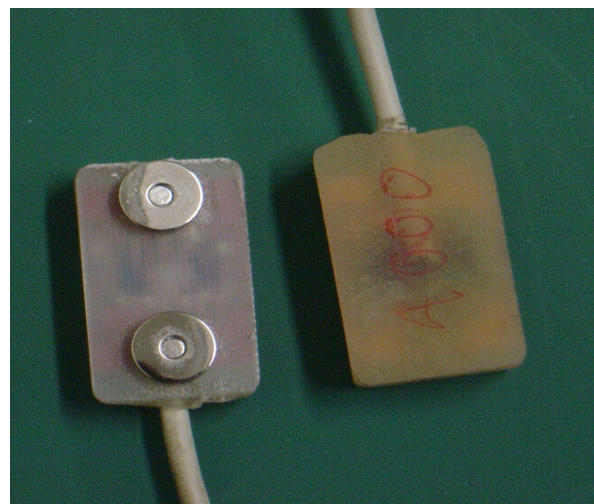


sEMG Electrode

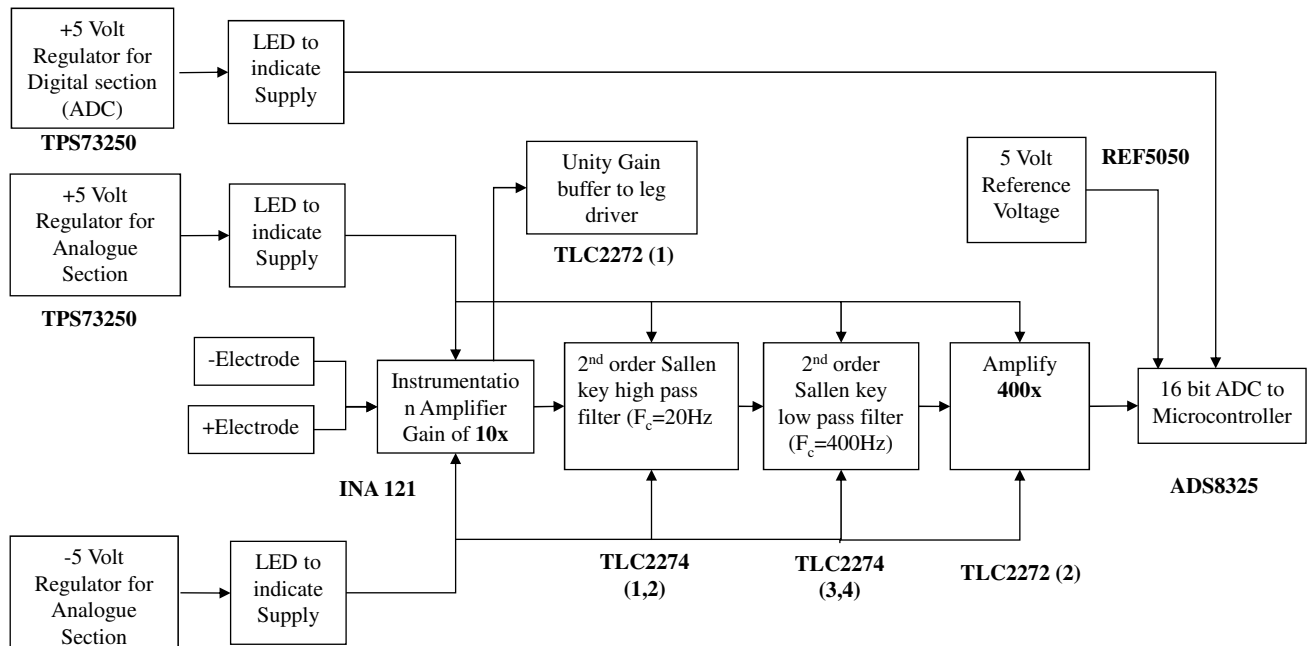


Initial Prototype

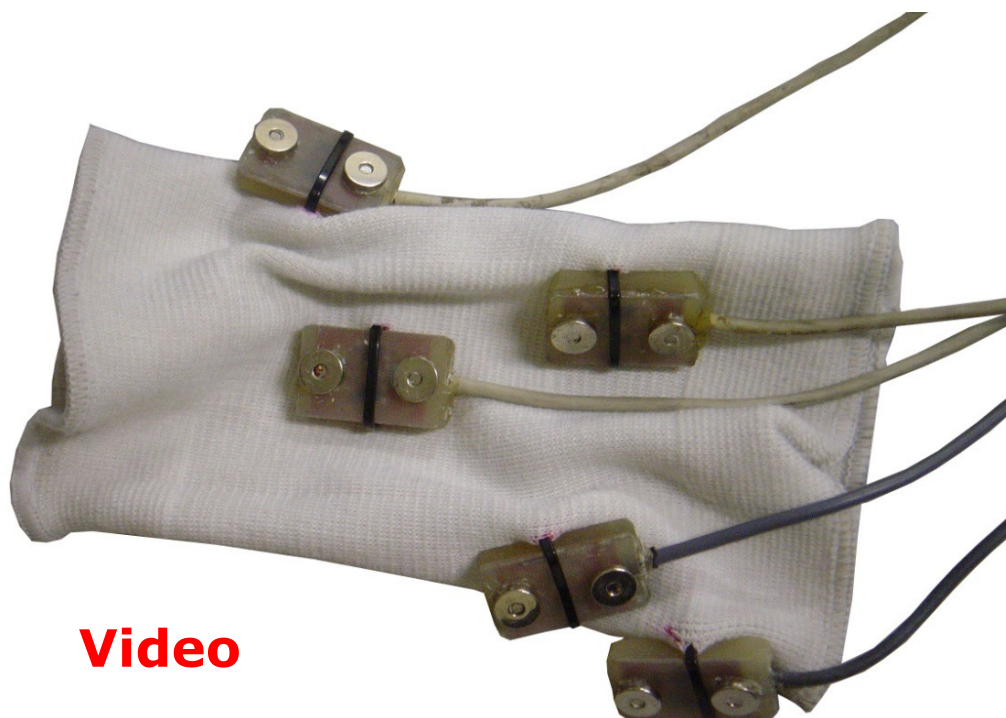
Final design



sEMG Signal Conditioning - Block Diagram



sEMG System

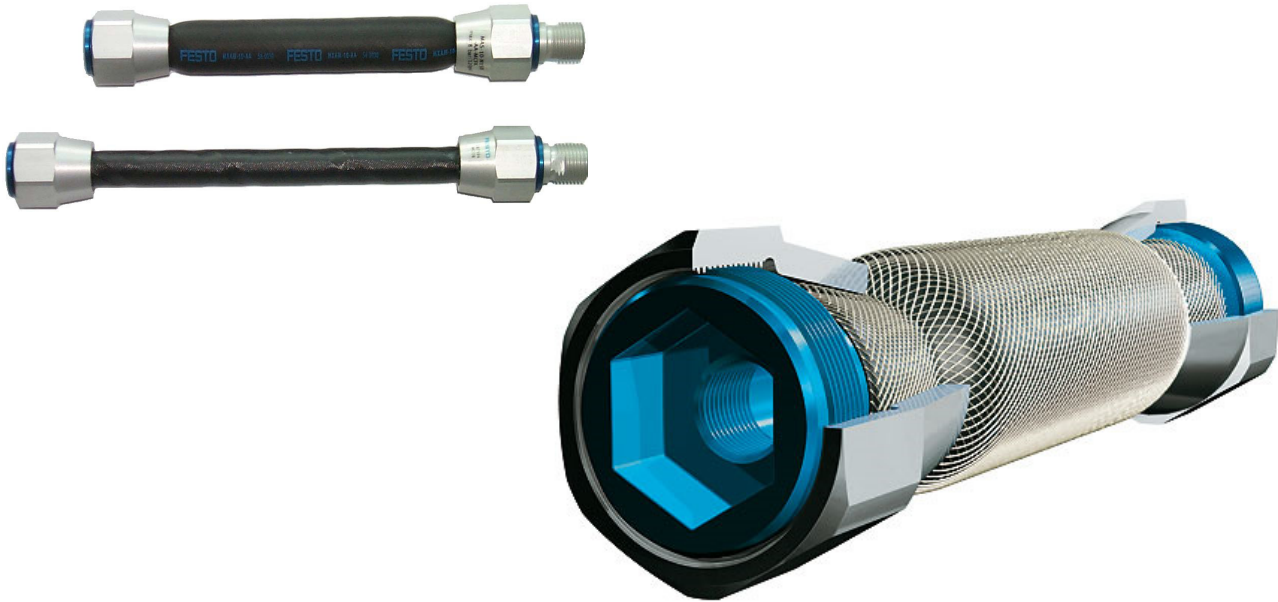


Video

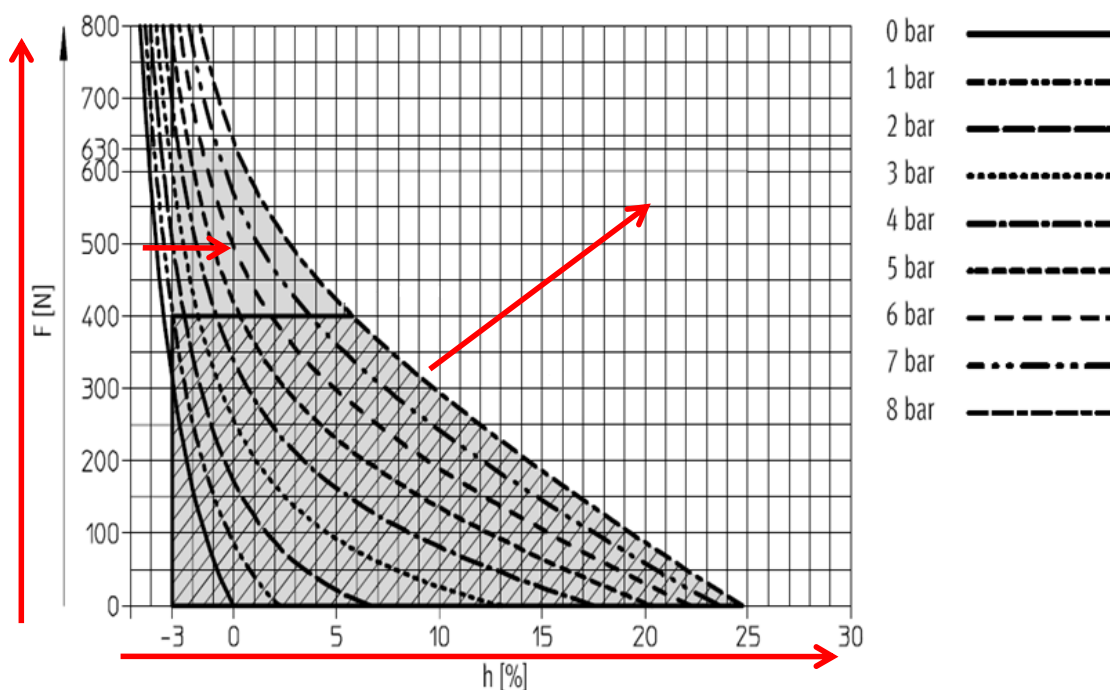


Actuation-Pneumatic Artificial Muscle (PAM)

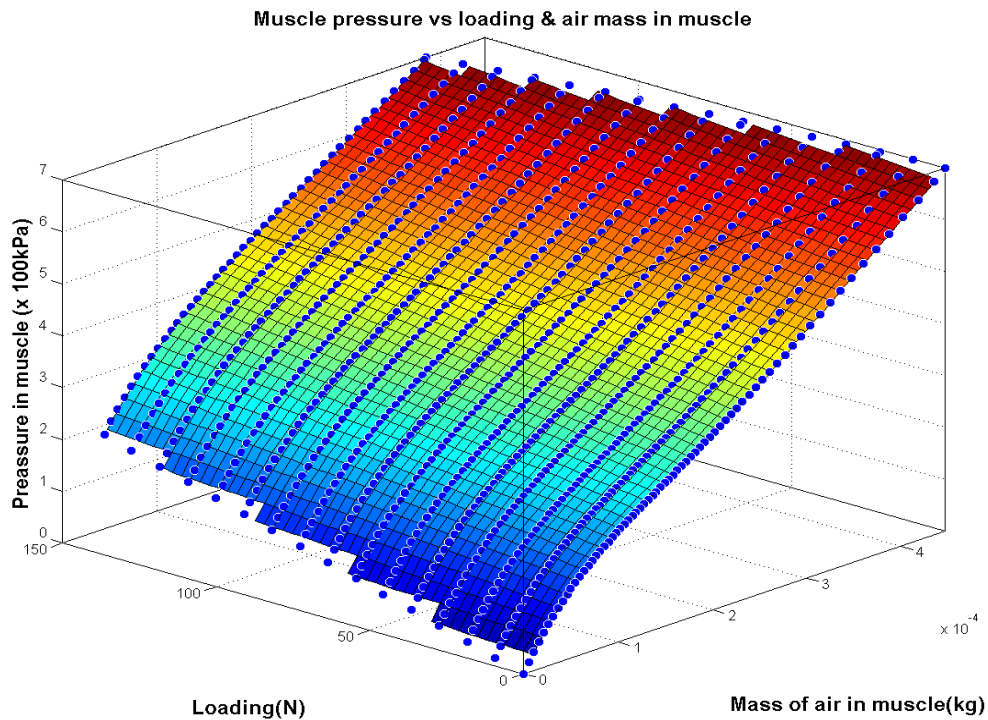
- Classical model: mesh angle
- Lumped mass model: Nonlinear spring & damper
- Characteristic look up table



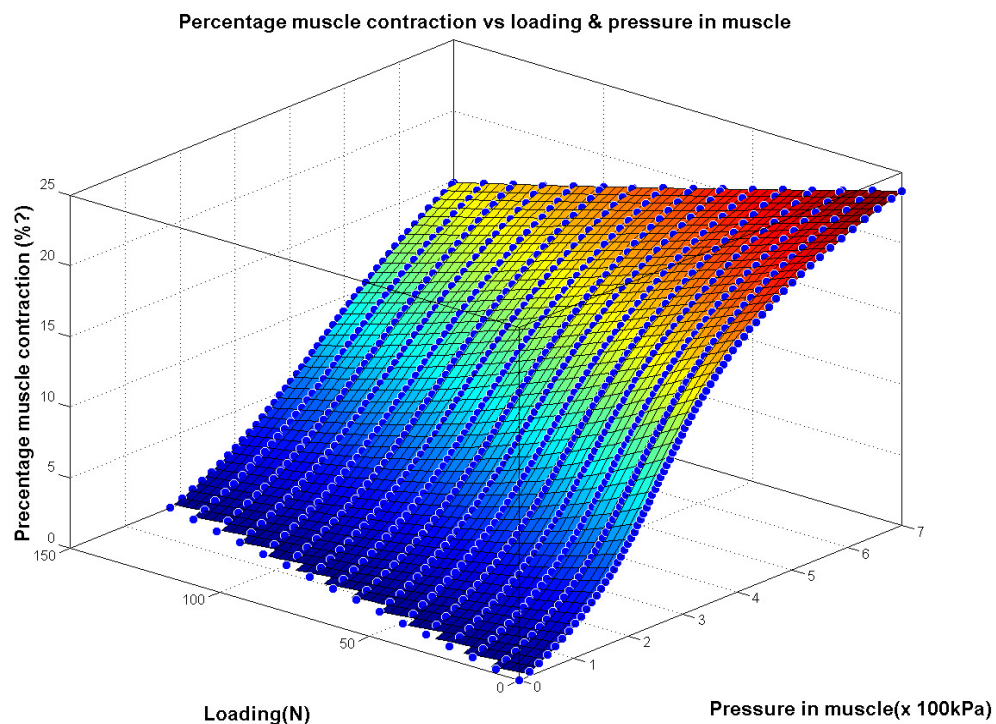
PAM Characteristics



PAM Modeling- Characteristic Surface



PAM Characteristic Surface

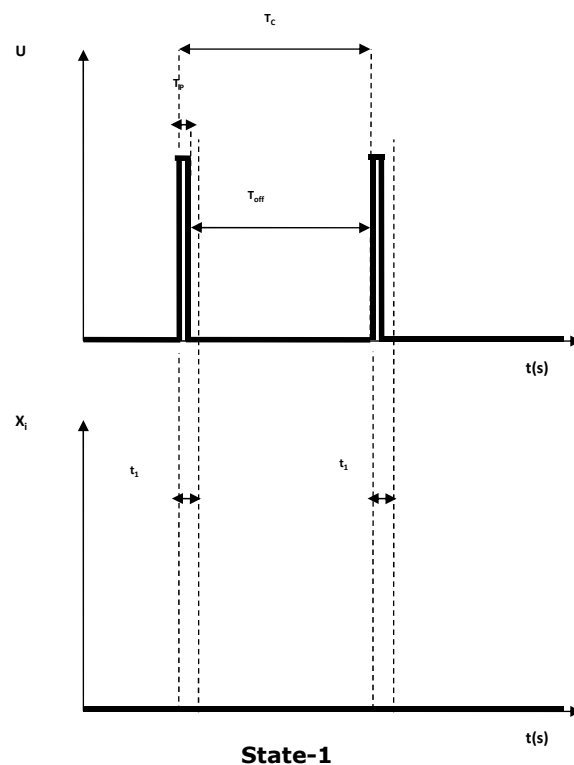
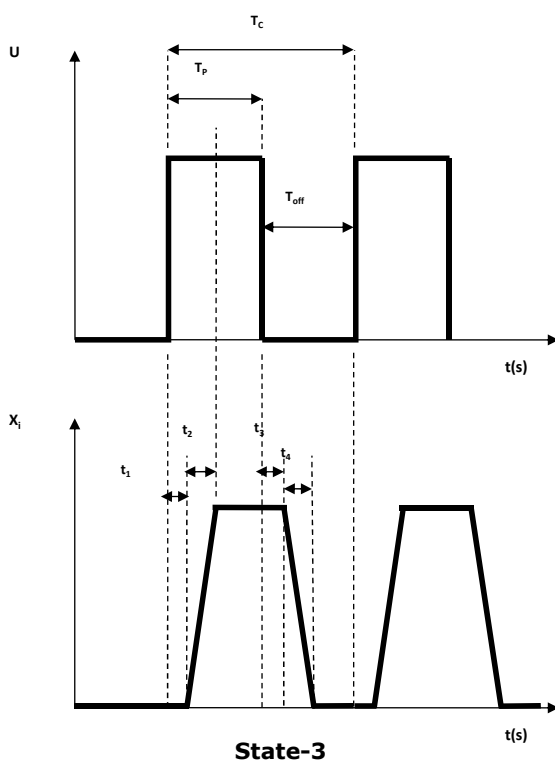


Mass flow rate of air

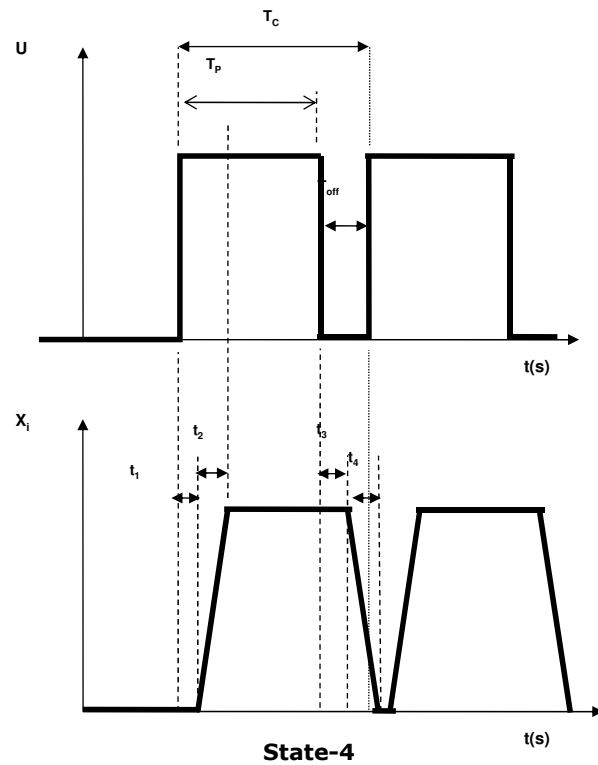
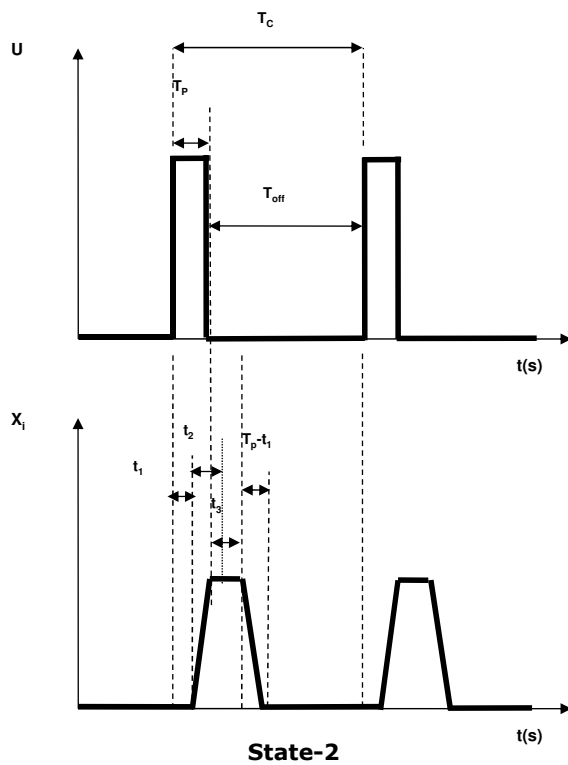
$$\dot{m} = \begin{cases} C_f \cancel{A_v} C_1 \frac{P_u}{\sqrt{T}} & \text{if } \frac{P_d}{P_u} \leq P_{cr} \\ C_f \cancel{A_v} C_2 \frac{P_u}{\sqrt{T}} \left(\frac{P_d}{P_u} \right)^{\kappa-1} \sqrt{1 - \left(\frac{P_d}{P_u} \right)^{\frac{\kappa-1}{\kappa}}} & \text{if } \frac{P_d}{P_u} > P_{cr} \end{cases}$$

$$C_1 = \sqrt{\frac{k}{R} \left(\frac{2}{\kappa + 1} \right)^{\frac{\kappa+1}{\kappa-1}}} \quad C_2 = \sqrt{\frac{k}{R} \left(\frac{2}{\kappa + 1} \right)} \quad P_{cr} = \left(\frac{2}{\kappa + 1} \right)^{\frac{\kappa}{\kappa-1}}$$

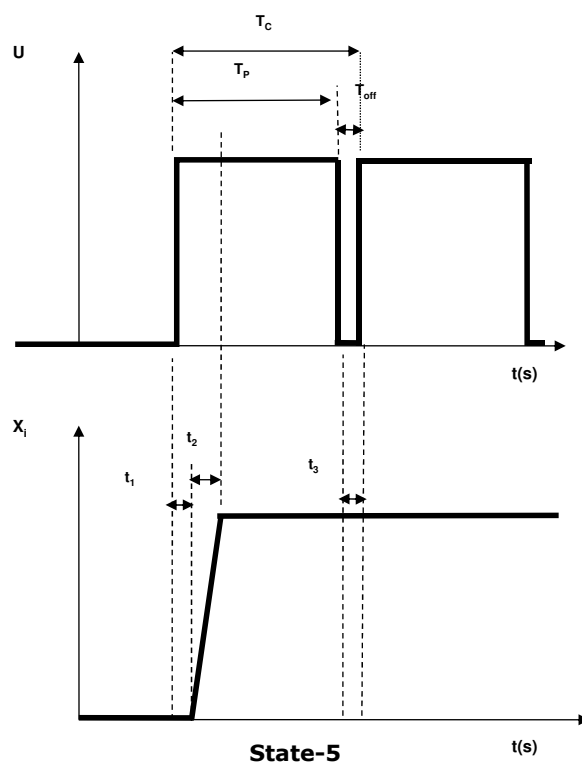
High Speed valve



High Speed valve



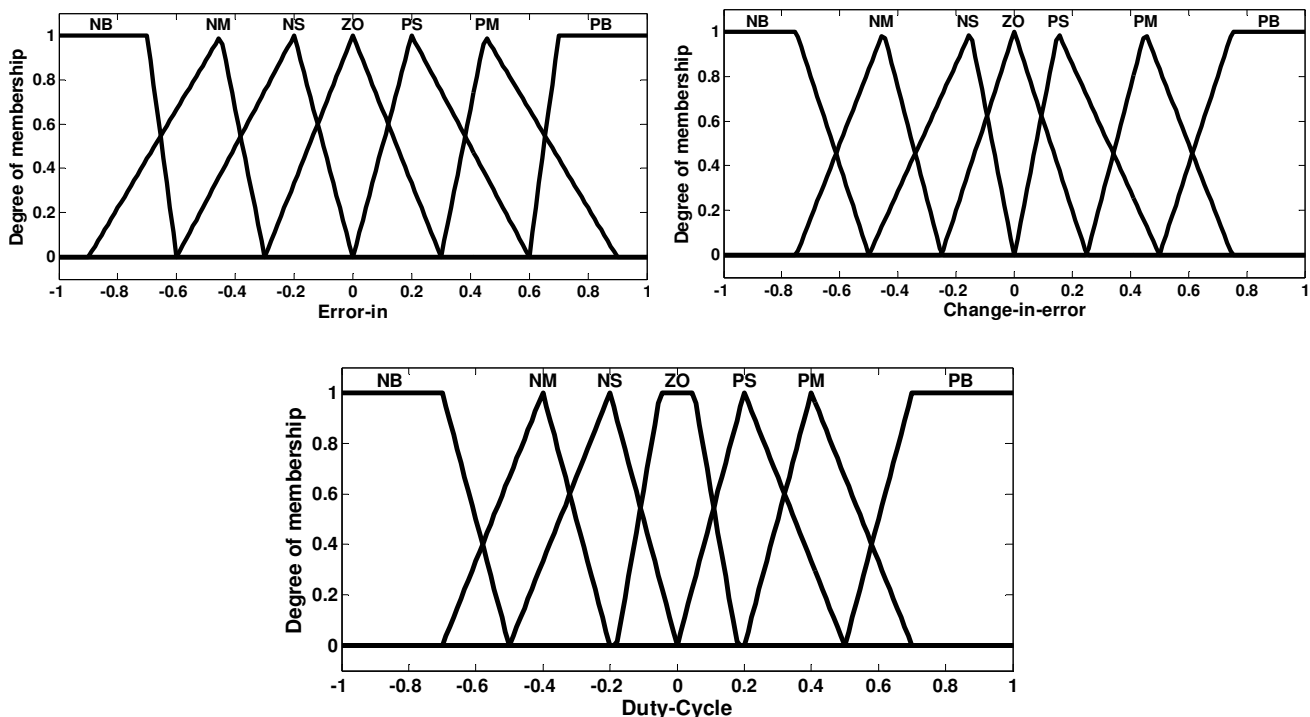
High Speed valve



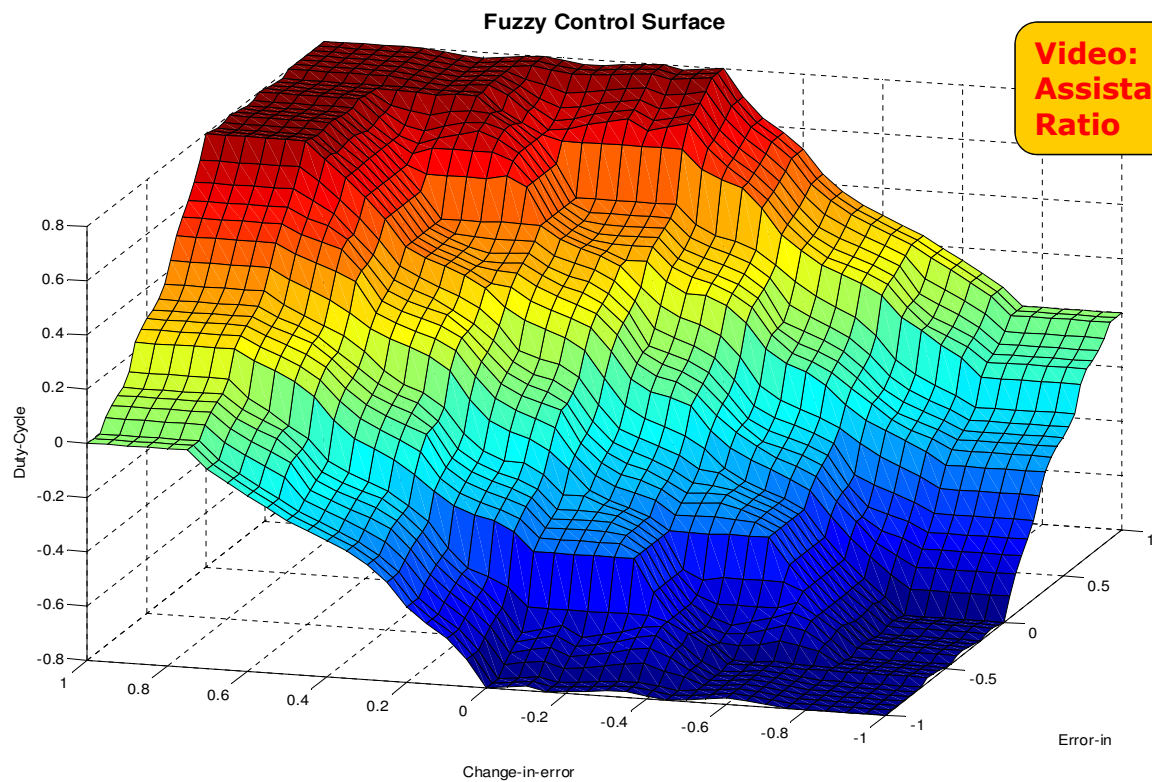
Fuzzy Logic Control

- Efficient Nonlinear Controller
- Model-less Controller
- Ability to compensate for variation and noise
- Existing knowledge from literature can be used in rule base
- Performance comparable to model based controller

Fuzzy Control-Variables



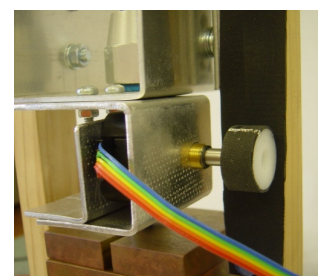
Fuzzy Control Surface



**Video:
Assistance
Ratio**

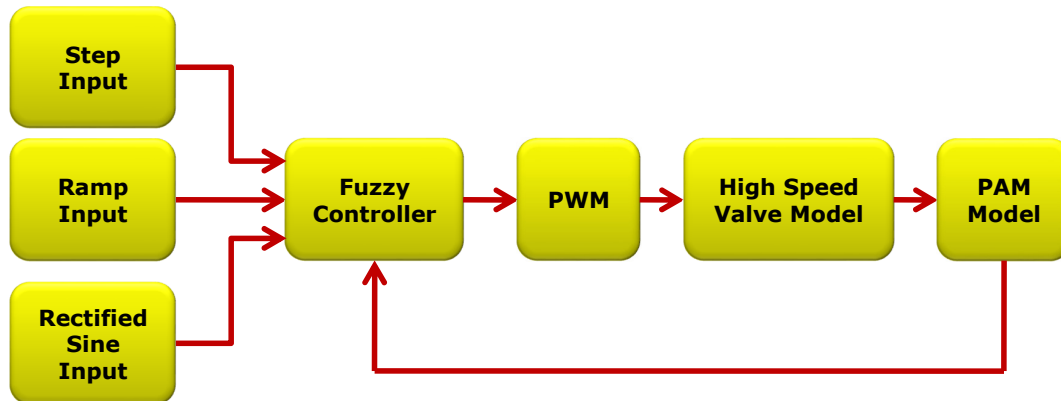


Experimental Setup

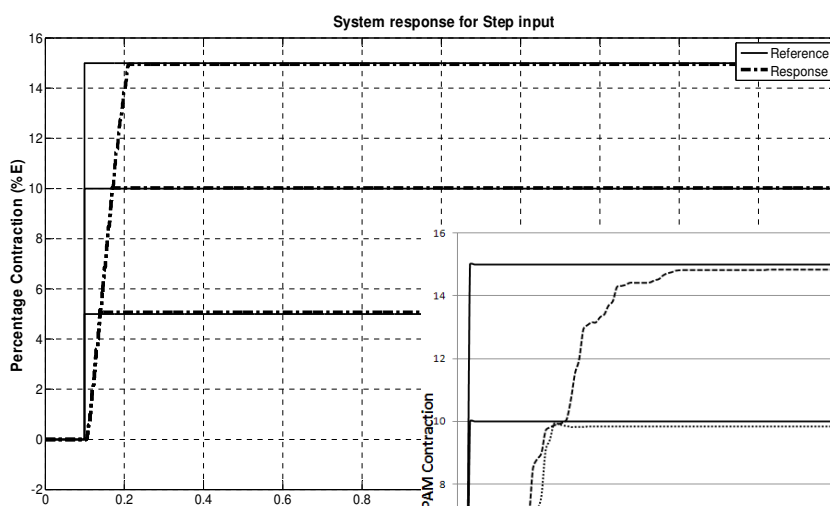


**5kg
Load**

Simulation Setup

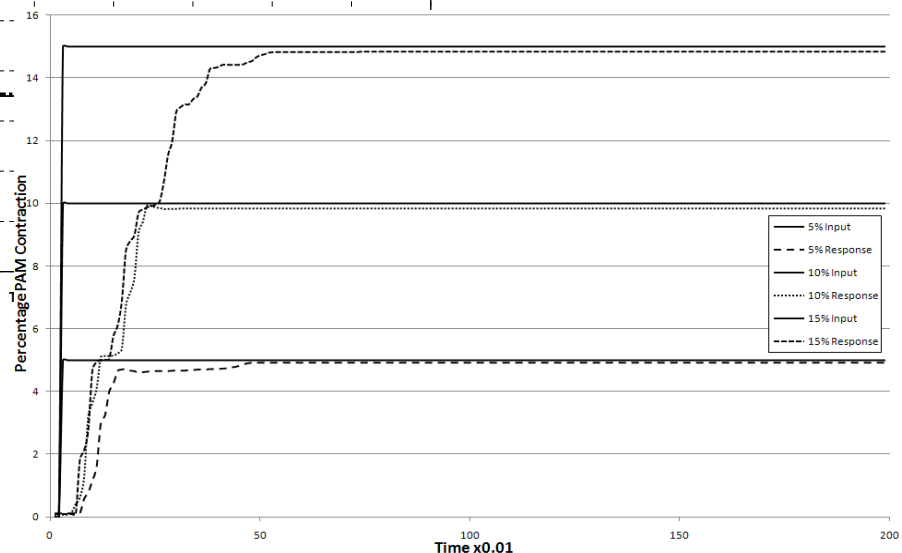


Results-Step Input

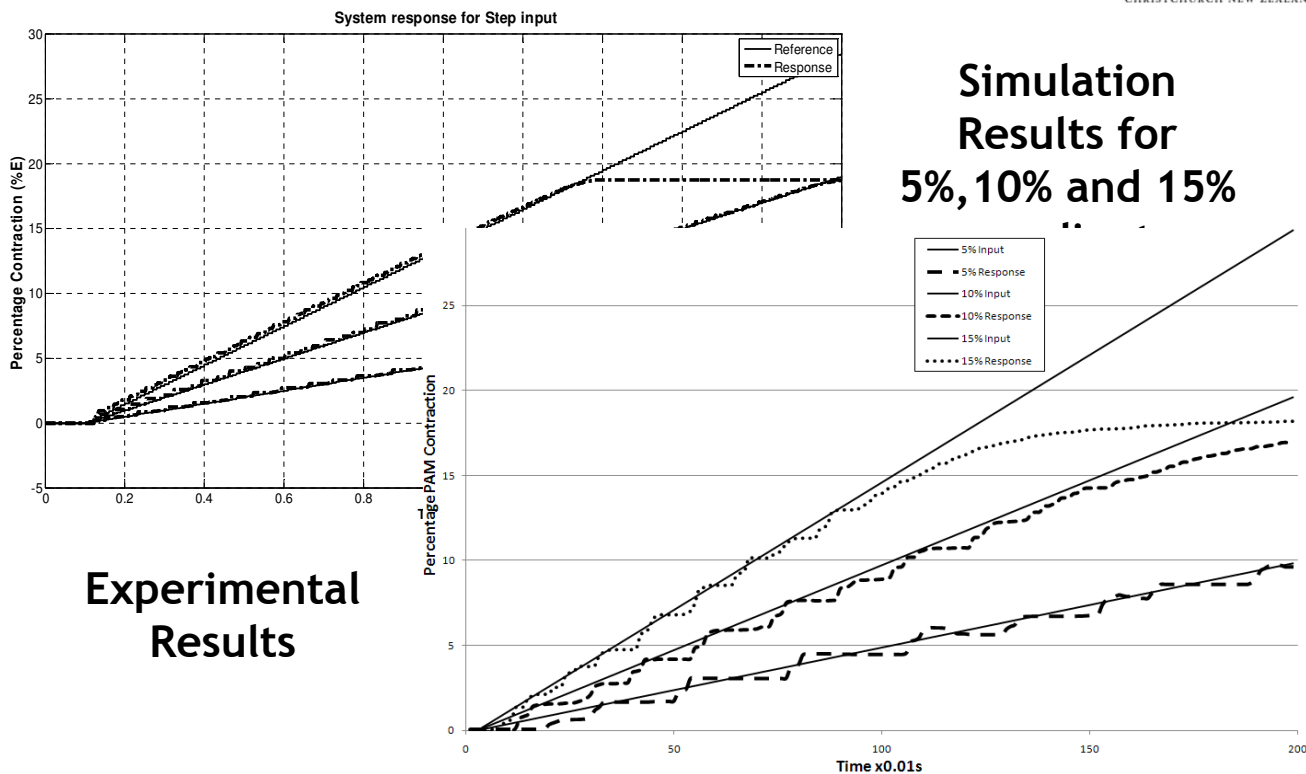


**Simulation Results
for 5%, 10% and
15%**

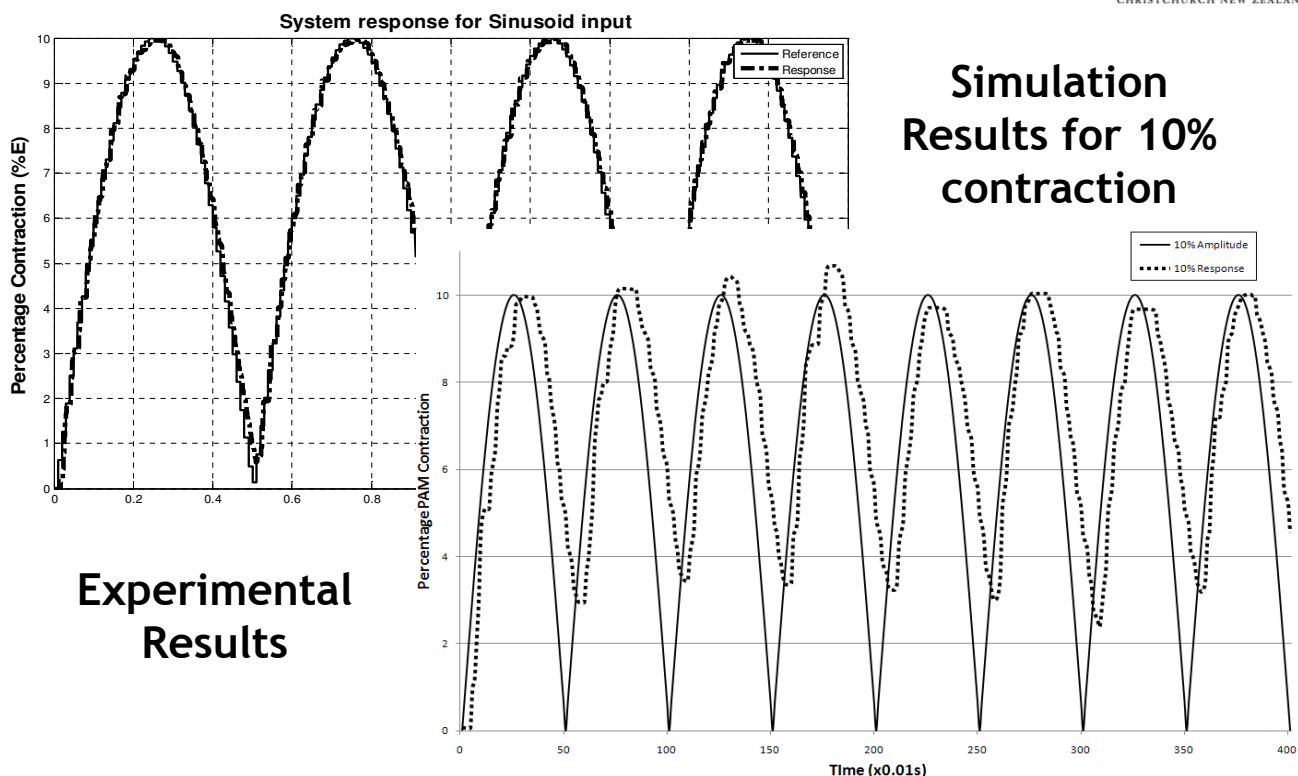
**Experimental
Results**



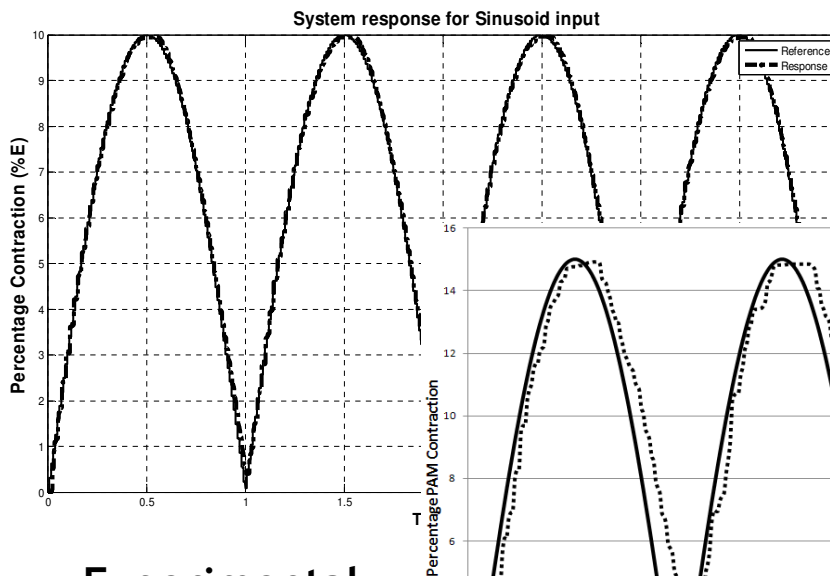
Results-Ramp Input



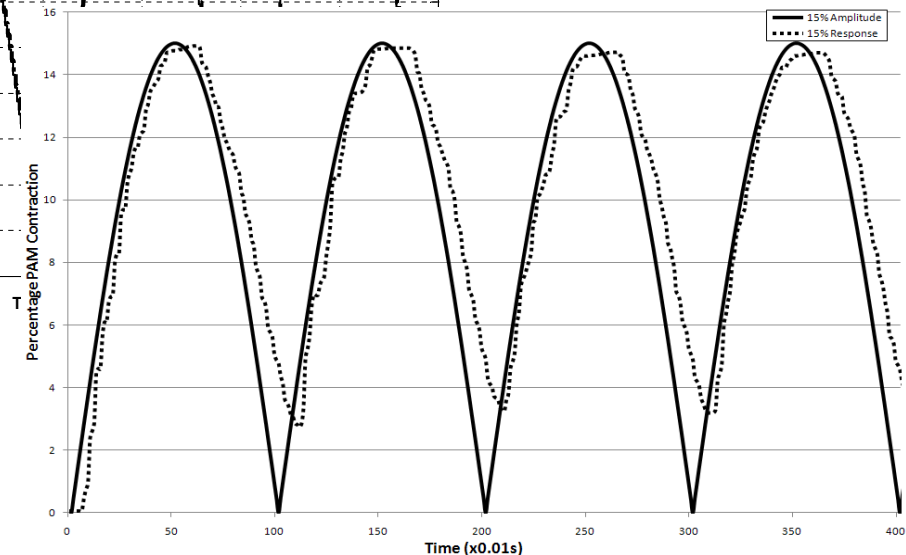
Results-2Hz Sine Input



Results-1Hz Sine Input



Experimental Results



Mark II: a lower limb exoskeleton

- Rehabilitative device for both medical and non-medical settings to assist the users leg muscles
- Aimed at people with walking difficulties but able to support themselves
- Encompasses ankle, knee and hip joints of both legs
- Actuation of knee and hip provided by pneumatic artificial muscles (PAM's)



Mark III: Soft exoskeleton velcro structure

Tightly in place; 2x PAM (pneumatic artificial muscle)

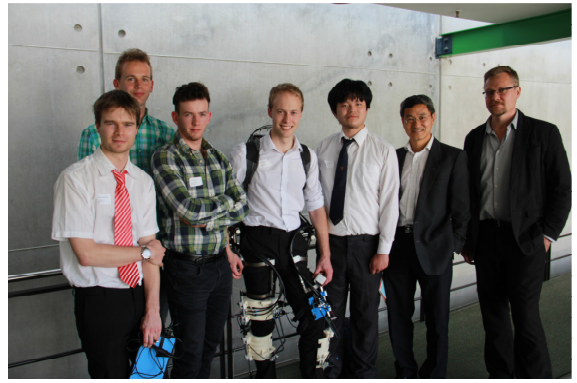


Conclusion

- Extract and process sEMG
- Design a soft exoskeleton
- Design self-organized fuzzy logic controller
- Validate controller performance
- Integrate the sEMG and controller into the exoskeleton

Acknowledgement

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- Intern: Vincent Groenhuis, University of Twente, Netherland
- Grant: KiwiNet
- Industry sponsor: Festo (New Zealand)



问 答 与 讨 论

